Exercise Stress Echocardiography of the Pulmonary Circulation

Limits of Normal and Sex Differences

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**Background:** Exercise stress echocardiography has not been recommended in the diagnostic workup of pulmonary hypertension because of insufficient certainty about feasibility and limits of normal.

**Methods:** Doppler echocardiography pulmonary hemodynamic measurements were performed at a progressively increased workload in 56 healthy male and 57 healthy female volunteers aged 19 to 63 years. Mean pulmonary artery pressure (mPAP) was estimated from the maximal tricuspid regurgitation jet velocity. Cardiac index was calculated from the left ventricular outflow velocity-time integral. Pulmonary vascular distensibility α index, the percentage change of vessel diameter per mm Hg of mPAP, was calculated from multipoint mPAP-cardiac output (CO) plots.

**Results:** Peak exercise at 175 ± 50 W was associated with an mPAP of 33 ± 7 mm Hg and a CO of 18 ± 5 L/min. The slope of mPAP-CO relationships was 1.5 ± 0.5 mm Hg/L/min, and the distensibility coefficient (α) was 1.3% ± 1.0%/mm Hg. Maximal workload and cardiac index were higher in men than in women (P < .05), but mPAP-cardiac index relationships were not different. However, women had a higher α (1.6% ± 1.3%/mm Hg vs 1.1% ± 0.6%/mm Hg, P < .05). The average mPAP-cardiac index slope was higher and α lower in subjects ≥ 50 years old. Upper limits of normal of mPAP at exercise were 34 mm Hg at a CO < 10 L/min, 45 mm Hg at a CO < 20 L/min, and 52 mm Hg at a CO < 30 L/min. These values are in keeping with previously reported invasive measurements.

**Conclusions:** Exercise stress echocardiography of the pulmonary circulation is feasible and allows for flow-corrected definition of upper limits of normal. Women have a more distensible pulmonary circulation.

**Abbreviations:** α = distensibility coefficient; CO = cardiac output; LAP = left atrial pressure; mPAP = mean pulmonary artery pressure; PAP = pulmonary artery pressure; PVR = pulmonary vascular resistance; sPAP = systolic pulmonary artery pressure

Pulmonary hypertension has been defined previously as a mean pulmonary artery pressure (mPAP) > 25 mm Hg at rest and > 30 mm Hg during exercise. Exercise measurements were withdrawn from the hemodynamic definition of pulmonary hypertension at an expert consensus conference held in 2008 in Dana Point. This decision was based mainly on an analysis of the reported invasive pulmonary hemodynamic studies in healthy subjects at exercise revealing uncertainty about the exact upper limits of normal. In the meantime, exercise-induced pulmonary arterial hypertension was validated as a clinical entity. Thus, a robust definition of the limits of normal of the pulmonary circulation at exercise would be of great relevance. However, for ethical and practical reasons, it is unlikely that a large number of rightsided heart catheterizations in healthy subjects will be reported in the near future. Therefore, there is currently interest in noninvasive exercise stress echocardiography of the pulmonary circulation.

We previously reported a preliminary study on the feasibility of noninvasive echo-Doppler measurements of the normal pulmonary circulation at rest and at exercise. From multipoint mPAP-flow coordinates in 25 healthy adults, we recovered pulmonary vascular resistance (PVR) and distensibility calculations...
that were in good agreement with those of previously reported invasive studies. We, therefore, now extend these measurements to a larger number of healthy men and women to define limits of normal and thereby offer a potentially useful test for the screening of people who are asymptomatic or mildly symptomatic with diseases associated with pulmonary hypertension.

**Materials and Methods**

One hundred twenty-four volunteers (62 women and 62 men) aged 37 ± 13 years (range, 18-63 years) with a height and weight of 173 ± 9 cm and 70 ± 11 kg, respectively (body surface area, 1.8 ± 0.2) gave an informed consent to the study, which was approved by the ethical committee of the Erasme University Hospital (No. P2011/101; Ref. EudraCT/CCB: B4006201110799, Brussels, Belgium). The subjects were nonsmokers and were free of any cardiovascular or lung disease. None had a family history of pulmonary hypertension. All were physically active, but none trained for >5 h per week, and, thus, were not considered athletes. Baseline clinical examination and ECG were normal. Eleven volunteers were excluded because of echocardiography of insufficient quality. Thus, complete sets of measurements were obtained in 57 women and 56 men. Forty-two women were taking oral contraceptives.

A standard echocardiographic examination was performed at rest and during exercise as reported previously. The workload was increased by 20 to 30 W every 2 min until the maximal workload tolerated because of dyspnea and/or leg pain. Echocardiographic measurements were taken during the last minute of each workload. Doppler echocardiography was performed with a Vivid ultrasound system (GE Healthcare) on a semirecumbent cycle ergometer (model 900 EL; Ergoline). The exercise table was tilted laterally by 20° to 30° to the left. Cardiac output (CO) was estimated from the left ventricular outflow tract cross-sectional area and pulsed Doppler velocity-time integral measurements.

Systolic pulmonary artery pressure (sPAP) was estimated from a trans-tricuspid gradient calculated from the maximal velocity (V) of continuous Doppler tricuspid regurgitation as 4 × V2 + 5 mm Hg assigned to right atrial pressure. mPAP was calculated as 0.6 × sPAP + 2.10 Left atrial pressure (LAP) was estimated from the ratio of Doppler mitral E flow-velocity wave and tissue Doppler mitral annulus flow E' early diastolic velocity (ie, LAP = 1.9 + 1.24 E/E').

The echocardiographic recordings were stored on optical disks and read in duplicate by blinded observers (P. A., M. D., and M. M.). We previously reported intraobserver variabilities for sPAP and CO estimates of 4.3% and 4.0% at rest and 8.2% and 7.7% at maximal exercise, respectively, and interobserver variabilities of sPAP and CO estimates of 1.9% and 4.9% at rest and 7.9% and 13.9% at maximal exercise, respectively. PVR was calculated as (mPAP – LAP)/CO. Multipoint mPAP-CO and mPAP-indexed CO (cardiac index) plots were tested for linearity, and linear regressions were calculated for pooled male and female measurements after Poorn adjustment for individual variability. Each multipoint mPAP-CO plot was also fitted to the equation:

\[
mPAP = \frac{\left(1 + aLAP\right)^3 + 5aR_s(CO)\right)^2 - 1}{\alpha}
\]

where \(R_s\) is the total PVR at rest, to calculate a distensibility \(\alpha\) index in percentage change in diameter per mm Hg increase in transmural pressure. To investigate the effect of exercise on the distensibility index, a specific distensibility coefficient (\(\alpha\)) index was calculated at rest (\(\alpha\)-rest) as well as at peak exercise (\(\alpha\)-peak). Results are presented as mean ± SD. The statistical analysis consisted of least-squares linear regression calculations and Student t tests after checking for normality of distributions using the D’Agostino skewness test. Nonnormal distributions were found in calculations of \(\alpha\) and slopes of pressure-flow curves, so a Wilcoxon rank sum test was performed. \(P < .05\) was considered significant. Limits of normal on slopes of mPAP-CO and mPAP-cardiac index were defined as mean ± 2 SD to mean + 2 SD. Prediction bands (S-pred) were calculated based on a quadratic fit of the pooled pressure-flow data in MATLAB (The MathWorks, Inc), using the equation:

\[
S_{\text{pred}}(x) = \sqrt{\frac{1}{n}\sum (x - \bar{x})^2}
\]

Statistical analysis was performed using R (R-project.org, version 2.13.0).

**Results**

Good-quality signals were available at all levels of exercise in all subjects. Because 11 subjects had been excluded at an initial echocardiographic evaluation, this corresponds to an 87% recovery rate of a complete exercise stress echocardiography of the pulmonary circulation in healthy adults.

**Pressure-Flow Relationships and Limits of Normal**

As shown in Table 1, peak exercise at an average of 175 W (men + women) was accompanied by a close-to-fourfold increase in CO and a doubling of mPAP. Exercise increased LAP by an average of 2 mm Hg and did not affect PVR. Each mPAP-CO plot was well

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Original Research

34 mm Hg at a CO below 10 L/min, 40 mm Hg at a CO of 15 L/min, 45 mm Hg at a CO of 20 L/min, and 52 mm Hg at a CO of 30 L/min.

CO was expectedly correlated to workload. However, as illustrated in Figure 2, there was a wide range of CO for any given level of workload.

Sex Differences

Comparisons between male and female subjects are presented in Tables 1 and 2. The men and women were of a similar average age, and the women had a lower body surface area. Resting mPAP was the same, but both CO and cardiac index were higher in men, whereas PVR, not indexed PVR, was higher in women (Table 1). The upper limit of normal of resting mPAP calculated as mean mPAP + 2 SD was 21 mm Hg in

Data are presented as mean ± SD. The average age in both the male and female group was similar, with 11 women and 14 men ± 50 years old.

CO = cardiac output; LAP = left atrial pressure; mPAP = mean pulmonary artery pressure; PVR = pulmonary vascular resistance; PVRi = indexed pulmonary vascular resistance; α = distensibility coefficient.

a P < .001 compared with men.
b P < .01 compared with men.
c Or mm Hg/min/L.
d P < .05 compared with men.

described by a linear approximation, with average correlation coefficients of 0.92 and an SD of 0.08. The average slope of mPAP-CO was 1.51 ± 0.54 mm Hg/L/min. After Poon adjustment, the average slope of a line best fit to pooled data was 1.46 mm Hg/L/min and the intercept 8 mm Hg. The mPAP-CO relationships were actually slightly curvilinear and, accordingly, also well fitted by the distensibility equation. The average distensibility coefficient α was 1.3% ± 1.0%/mm Hg but it decreased by approximately 50% from rest to maximal exercise.

The limits of normal of the slopes of multipoint mPAP-CO relationships calculated as mean ± 2 SD to mean + 2 SD were 0.5 to 2.5 mm Hg/L/min. Limits of normal of prediction bands for mPAP-CO relationships are shown in Figure 1. This presentation shows that the upper limit of normal of mPAP would be 34 mm Hg at a CO below 10 L/min, 40 mm Hg at a CO of 15 L/min, 45 mm Hg at a CO of 20 L/min, and 52 mm Hg at a CO of 30 L/min.

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**Sex Differences**

Comparisons between male and female subjects are presented in Tables 1 and 2. The men and women were of a similar average age, and the women had a lower body surface area. Resting mPAP was the same, but both CO and cardiac index were higher in men, whereas PVR, not indexed PVR, was higher in women (Table 1). The upper limit of normal of resting mPAP calculated as mean mPAP + 2 SD was 21 mm Hg in

![Image](image-url)

**Figure 1.** A, Mean pulmonary artery pressure (mPAP)-cardiac output (CO) relationships at rest and at progressively increased workloads. The prediction band is shown by the shaded area. mPAPs at CO values of 10, 20, and 30 L/min are shown by the stippled lines. B, Poon-adjusted linear fit of the data points to recover a “normal” slope of 1.46 mm Hg/L/min.
both men and women. At peak exercise, men achieved higher maximal workload, CO, cardiac index, and mPAP, whereas PVR or indexed PVR were not different. There was a slight increase in LAP, by an average of 2 mm Hg, at maximal exercise, which was not different in women and in men. The upper limits of normal of mPAP at exercise were 48 mm Hg in men and 45 mm Hg in women. mPAP-CO or mPAP-cardiac index relationships were not different between men and women (Table 2). This was confirmed by the slopes of the linear fit to the Poon-adjusted mPAP-CO and mPAP-cardiac index data (Fig 3). As also shown in Table 1, sex had no measurable effect on $\alpha$ at rest, but at peak exercise $\alpha$ was significantly less in men.

In the women, $\alpha$ decreased as a function of age ($-0.025%/\text{mm Hg/yr}, R^2 = 0.07$), down to values indiscernible from men at $\geq 50$ years (Table 2).

**Age Differences**

Twenty-five subjects, 11 women and 14 men, were $\geq 50$ years old. Their characteristics and hemodynamic measurements, compared with those of subjects $< 50$ years old, are presented in Tables 3 and 4. Older subjects had slightly higher mPAP and LAP at rest, lower maximal workload and cardiac index, steeper slopes of mPAP-CO or mPAP-cardiac index plots, and a trend to lower $\alpha$. PVR was not different. Steeper slopes of Poon-adjusted mPAP-cardiac index relationships in older subjects are illustrated in Figure 4.

**Discussion**

The results show that the upper limits of normal for mPAP at stress echocardiography depend on the achieved maximal CO. The previously used cut-off value of 30 mm Hg for the diagnosis of exercise-induced pulmonary hypertension is accurate for a CO below 8 to 10 L/min. Higher upper limits of normal for exercise mPAP, up to 50 mm Hg, are to be considered for higher COs achieved by fit healthy subjects. The results also show, we believe for the first time, that there are no sex differences in PVR, but there is a higher pulmonary vascular distensibility in women $\geq 50$ years old. Limited data on a small subgroup of subjects $\geq 50$ years old reveal expected steeper pulmonary vascular pressure-flow relationships and decreased distensibility.

Exercise stress echocardiographic measurements of the pulmonary circulation are usually reported as single sPAP estimates with or without mention of the achieved workload. This approach has indicated a higher prevalence of higher-than-normal exercise sPAP in the relatives of patients with pulmonary arterial hypertension as compared with control subjects. In these studies, the upper limit of normal of sPAP at exercise was estimated to be around 40 mm Hg. However, the same upper limit of normal has been determined for resting aging and overweight subjects or resting young adult athletes. This could be explained by altered left ventricular diastolic function with aging and obesity and by increased stroke volume as a result of training. It has long been believed that pulmonary artery pressure (PAP) does not increase much with exercise, so that an mPAP $> 30$ mm Hg (corresponding to an sPAP of 47 mm Hg) at exercise would definitely be diagnostic of pulmonary vascular disease. However, mPAP increases at high levels of exercise, up to values of around 40 to 50 mm Hg as reported in invasive, as well as noninvasive studies. In the

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**Table 2—Characteristics of 56 Male and 57 Female Subjects**

<table>
<thead>
<tr>
<th>Variable</th>
<th>Men</th>
<th>Women</th>
</tr>
</thead>
<tbody>
<tr>
<td>Age, y</td>
<td>38 ± 14</td>
<td>37 ± 13</td>
</tr>
<tr>
<td>BSA, m²</td>
<td>2.0 ± 0.1</td>
<td>1.7 ± 0.1</td>
</tr>
<tr>
<td>mPAP-CO, mm Hg/L/min</td>
<td>1.46 ± 0.48</td>
<td>1.55 ± 0.60</td>
</tr>
<tr>
<td>mPAP-cardiac index, mm Hg/L/min/m²</td>
<td>2.9 ± 0.9</td>
<td>2.6 ± 1</td>
</tr>
<tr>
<td>Poon mPAP-CO, mm Hg/L/min</td>
<td>1.40</td>
<td>1.51</td>
</tr>
<tr>
<td>$\alpha$, %/mm Hg</td>
<td>1.1 ± 0.6</td>
<td>1.6 ± 1.3</td>
</tr>
<tr>
<td>$&lt; 50$ y</td>
<td>1.0 ± 0.6</td>
<td>1.7 ± 1.4</td>
</tr>
<tr>
<td>$\geq 50$ y</td>
<td>1.1 ± 0.6</td>
<td>1.0 ± 0.3</td>
</tr>
<tr>
<td>Maximal workload, W</td>
<td>198 ± 54</td>
<td>153 ± 34</td>
</tr>
</tbody>
</table>

Data are presented as mean ± SD unless indicated otherwise. BSA = body surface area. See Table 1 for expansion of other abbreviations. $^aP<.001$ compared with men. $^bP<.01$ compared with men.
assumptions in the calculations of vascular pressures and volume flows. Quality control studies have reported a disappointingly poor agreement between sPAP estimated from the maximal velocity of tricuspid regurgitation and invasive measurements at right-sided heart catheterization. CO calculated from the left ventricular outflow tract dimension and velocity-time integral tends to be underestimated, mainly because of the underestimation of left ventricular outflow tract dimensions. However, although this is not proof, it may be noted that in the present study the Doppler echocardiographic measurements of mPAP and CO were in good agreement with previous invasive studies at any given level of workload.

Echocardiographic estimates of pulmonary vascular pressures and CO are advantageous because they are noninvasive and flexible but have to rely on a series of assumptions in the calculations of vascular pressures and volume flows. Quality control studies have reported a disappointingly poor agreement between sPAP estimated from the maximal velocity of tricuspid regurgitation and invasive measurements at right-sided heart catheterization. CO calculated from the left ventricular outflow tract dimension and velocity-time integral tends to be underestimated, mainly because of the underestimation of left ventricular outflow tract dimensions. However, although this is not proof, it may be noted that in the present study the Doppler echocardiographic measurements of mPAP and CO were in good agreement with previous invasive studies at any given level of workload.

Table 3—Hemodynamic Measurements at Rest and at Peak Exercise of 25 Subjects <50 Years Old Compared With 88 Subjects ≥50 Years Old

<table>
<thead>
<tr>
<th>Characteristic</th>
<th>&lt;50 y</th>
<th>Peak Exercise</th>
<th>≥50 y</th>
<th>Peak Exercise</th>
</tr>
</thead>
<tbody>
<tr>
<td>mPAP, mm Hg</td>
<td>14.9 ± 2.5</td>
<td>32.4 ± 7.4</td>
<td>17.0 ± 3.0</td>
<td>35.9 ± 5.3</td>
</tr>
<tr>
<td>LAP, mm Hg</td>
<td>7.7 ± 1.3</td>
<td>9.5 ± 1.3</td>
<td>9.0 ± 1.0</td>
<td>11.0 ± 0.8</td>
</tr>
<tr>
<td>CO, L/min</td>
<td>5.2 ± 1.4</td>
<td>18.1 ± 4.9</td>
<td>5.2 ± 1.1</td>
<td>16.0 ± 3.2</td>
</tr>
<tr>
<td>Cardiac index, L/min/m²</td>
<td>2.95 ± 0.56</td>
<td>9.8 ± 2.1</td>
<td>2.77 ± 0.57</td>
<td>8.5 ± 1.5</td>
</tr>
<tr>
<td>PVR, Woods units⁴</td>
<td>1.42 ± 0.59</td>
<td>1.28 ± 0.35</td>
<td>1.61 ± 0.83</td>
<td>1.61 ± 0.47</td>
</tr>
<tr>
<td>PVR, Woods units⁴/m²</td>
<td>2.6 ± 1.0</td>
<td>2.3 ± 0.6</td>
<td>3.0 ± 1.5</td>
<td>3.0 ± 0.8</td>
</tr>
<tr>
<td>α, %/mm Hg</td>
<td>2.2 ± 1.6</td>
<td>1.3 ± 0.9</td>
<td>2.0 ± 1.7</td>
<td>0.9 ± 0.3</td>
</tr>
</tbody>
</table>

See Table 1 for expansion of abbreviations.

<sup>a</sup>P < .001 compared with subjects <50 years old.
<sup>b</sup>P < .05 compared with subjects <50 years old.
<sup>c</sup>P < .01 compared with subjects <50 years old.
<sup>d</sup>Or mm Hg/min/L.
Table 4—Characteristics of 25 Subjects ≥ 50 Years Old Compared With 88 Subjects < 50 Years Old

<table>
<thead>
<tr>
<th>Variable</th>
<th>&lt; 50 y</th>
<th>≥ 50 y</th>
</tr>
</thead>
<tbody>
<tr>
<td>Age, y</td>
<td>32 ± 9</td>
<td>57 ± 4*</td>
</tr>
<tr>
<td>BSA, m²</td>
<td>1.82 ± 0.2</td>
<td>1.88 ± 0.14*</td>
</tr>
<tr>
<td>mPAP-CO, mm Hg/L/min</td>
<td>1.40 ± 0.46</td>
<td>1.88 ± 0.65*</td>
</tr>
<tr>
<td>Cardiac index, mm Hg/L/min/m²</td>
<td>2.5 ± 0.8</td>
<td>3.5 ± 1.2*</td>
</tr>
<tr>
<td>Intercept</td>
<td>8.2 ± 4.0</td>
<td>7.4 ± 5.0</td>
</tr>
<tr>
<td>α, %/mm Hg</td>
<td>1.4 ± 1.1</td>
<td>1.1 ± 0.5</td>
</tr>
<tr>
<td>Maximal workload, W</td>
<td>180 ± 49</td>
<td>159 ± 53*</td>
</tr>
</tbody>
</table>

See Tables 1 and 2 for expansion of abbreviations.

*P < .001 compared with subjects < 50 years old.

**P < .05 compared with subjects < 50 years old.

Errors on measurements. The weakest measurement from a methodologic point of view in the present study would probably be LAP estimated from an E/E’ ratio, which could explain why LAP did not increase at the highest level of exercise, as expected. Previous validation studies of E/E’ to estimate LAP or wedge PAP reported excessively high cardiac indexes and an absence of linear relationship between E/E’ and wedge PAP at exercise. However, wedge PAP has also been shown to correlate poorly with left ventricular end-diastolic pressures, so invasively measured wedge PAP might not be an optimal gold standard for noninvasive estimates of LAP. Furthermore, mPAP-CO relationships at exercise show little change in LAP up to CO around 20 L/min, but a steep increase at higher CO, which is delayed to even higher CO in the most fit subjects. Thus, only a mild increase in LAP by an average of 2 mm Hg from rest to maximal exercise in the present study is not unexpected. It may be added that LAP is part of the α distensibility calculations, which yielded the expected range of values.

Because pulmonary vascular pressures are flow dependent, we defined the resistive properties of the pulmonary circulation by multipoint mPAP-CO or mPAP-cardiac index relationships. This approach has been shown repeatedly to allow for improved definition of PVR. We confirmed previously reported high levels of linear correlations between mPAP and flow at exercise, so these relationships could reasonably be described by linear approximations. Previously calculated mean slopes of mPAP-CO were of 1 mm Hg/L/min in young adults, increasing to 2.5 mm Hg/L/min in advanced age. The average slopes of mPAP-CO relationships in the present study on middle-aged adults stabilized at 1.5 mm Hg/L/min and, thus, were in keeping with these previous estimates from invasive measurements. However, because pulmonary resistive vessels are distensible, multipoint mPAP-CO plots are actually slightly curvilinear. It is possible to calculate a distensibility coefficient accounting for the recovered curvilinearity of mPAP-CO. Using a realistic distensibility model of the pulmonary circulation, an α value of approximately 2%/mm Hg has been calculated previously from invasive measurements in young adult volunteers. A distensibility of the same order of magnitude was calculated from the present noninvasive determinations, confirming the previous report. It is of interest that α decreased by approximately 50% from rest to exercise, in keeping with the notion that pulmonary

Figure 4. Poon-adjusted mPAP as a function of cardiac index at rest and at progressively increased workloads in healthy subjects. Aging was associated with an increased slope of the relationships. A, < 50 years. B, ≥ 50 years. See Figure 1 and 3 legends for expansion of abbreviations.
vascular compliance decreases along with increased distending pressures.

Previous exhaustive reviews of invasive pulmonary hemodynamic studies failed to uncover sex differences. This may be explained by the relatively small number of reported individual exercise measurements and the limited variable levels of workload and CO, making isoflow comparisons difficult. In the present study, the linear approximations of pulmonary vascular pressure-flow relationships were not different in men and women. However, when the pressure-flow coordinates were fitted to a distensibility model of the pulmonary circulation, it became apparent that women below the age of 50 years present with a higher pulmonary vascular compliance. In the present study, α was 45% higher in women than in men, but the sex difference disappeared in subjects ≥50 years old.

CO was lower in women than in men in the present study, which is in agreement with previous invasive measurements. Somewhat surprisingly, the difference persisted after correction for body size. Recent MRI measurements confirmed a lower CO in women, but this sex difference was not any more significant when corrected for body size, with a cardiac index around 3.0 L/min/m² for men and 2.8 L/min/m² for women. However, in these studies, body size-corrected right ventricular volume and mass were lower in women. The present results suggest that this may be due to the lower afterload of a more distensible pulmonary circulation.

The exercise stress tests were performed in a semi-recumbent position. Previous invasive studies reported a higher resting PVR in the upright, compared with recumbent, position, because of gravity-dependent lower venous return leading to pulmonary vascular derecruitment. However, the difference disappeared with exercise, in relation to increased pulmonary blood flow and full vascular recruitment. Accordingly, multipoint mPAP-CO relationships were not affected by body position. It is, therefore, unlikely that body position would have affected the stress echocardiography-derived pulmonary vascular pressure-flow relationships.

Our study was not designed to study the effects of aging on the pulmonary circulation. However, in 25 of the 113 subjects aged ≥50 years old, the slope of mPAP-cardiac index was increased and α was decreased, confirming previous estimations. The group of subjects ≥50 years old was too small, with the oldest subject aged 63 years, to allow for estimations of limits of normal as a function of increased aging. Nevertheless, it is remarkable that the present noninvasive measurements uncovered the expected effects of aging on resistive and distensibility properties of the pulmonary circulation.

There are several additional limitations to the present study. The recovery rate of 87% of sufficient-quality signals at the echocardiography of the pulmonary circulation of normal subjects is unusually high and is probably explained by high levels of previous training and the dedication of the investigators. Lower recovery rates may be expected in daily clinical practice. Furthermore, there was no validation against gold standard invasive measurements. However, this would be ethically and practically very difficult to obtain in a large number of healthy subjects. Finally, the study was performed in a single center and, thus, would require confirmation in a multicentric fashion.

In summary, the present results offer flow-corrected upper limits of normal of PAPs at exercise stress echocardiography that are compatible with previous invasive measurements. The results also show that women have a more distensible pulmonary circulation, which is likely estrogen related. It is hoped that improved definition of the limits of normal of exercise stress echocardiography estimates of pulmonary vascular pressures and CO will help make the method useful for the early diagnosis of pulmonary hypertension.

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**Author contributions:** Dr Argiento: contributed to the original design and concept of the study, data acquisition, data analysis, and preparation and critical review of the manuscript. Dr Vanderpool: contributed to the analysis and interpretation of data and preparation and critical review of the manuscript. Dr Mulè: contributed to the data acquisition, data analysis, review of echocardiographic images, and critical review of the manuscript. Dr Russo: contributed to the concept of the study and critical review of the manuscript. Dr D’Alto: contributed to the review of the echocardiographic images and critical review of the manuscript. Dr Bossone: contributed to the concept of the study and critical review of the manuscript. Dr Chesler: contributed to the data analysis and critical review of the manuscript. Dr Naeije: contributed to the overall design and concept of the study, analysis and interpretation of data, and preparation and critical review of the manuscript.

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**Other contributions:** This work was performed at the Free University of Brussels, Brussels, Belgium.

**References**


